

Imaging oxygenation by near-infrared optical tomography based on SPAD image sensors

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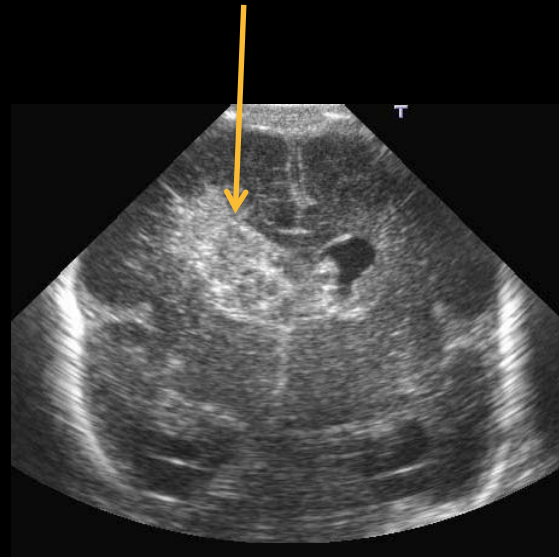


Brain lesions in preterm infants

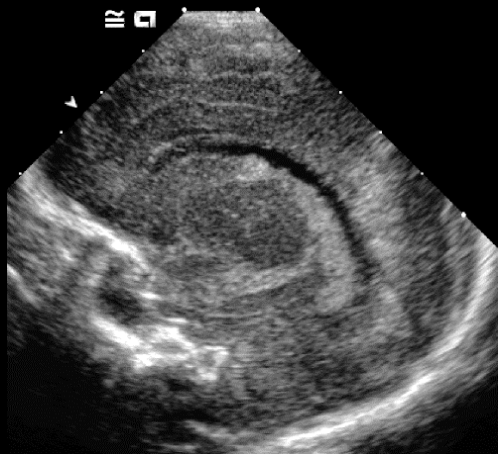
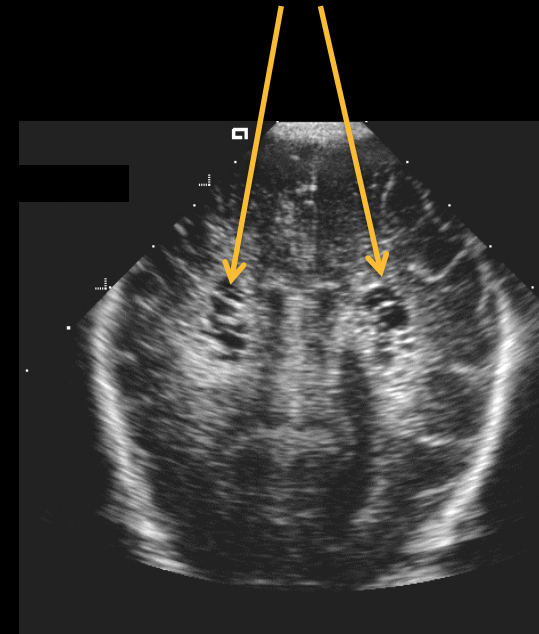
Healthy



Bleeding due to hypoxia



Cysts due to hypoxia/ischemia

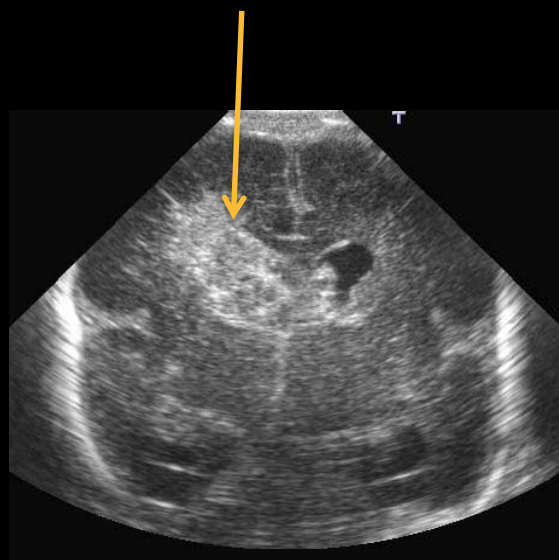


Brain lesions in preterm infants

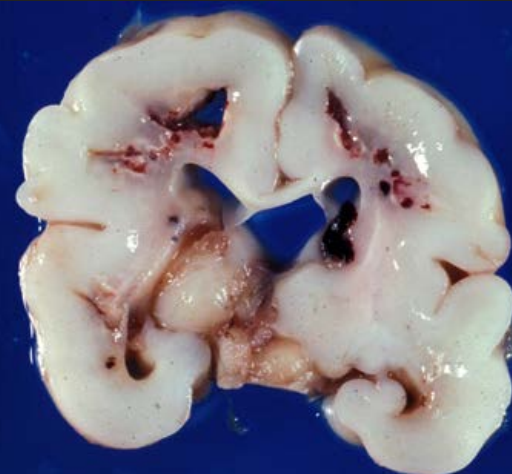
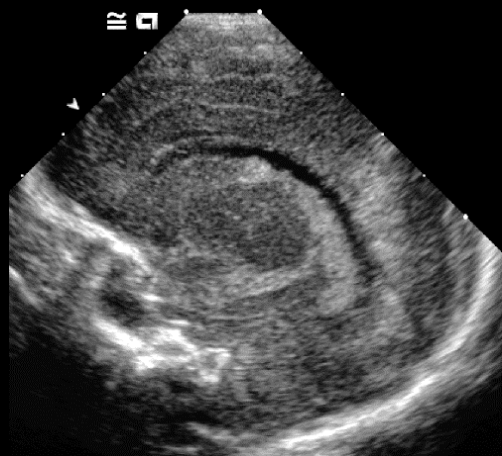
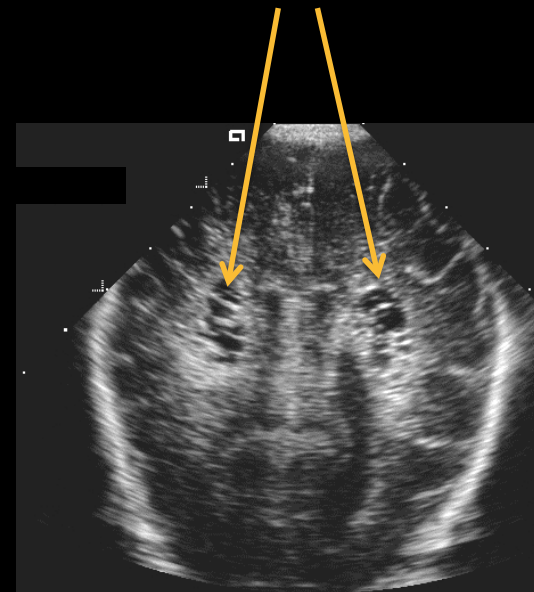
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Brain lesions in preterm infants

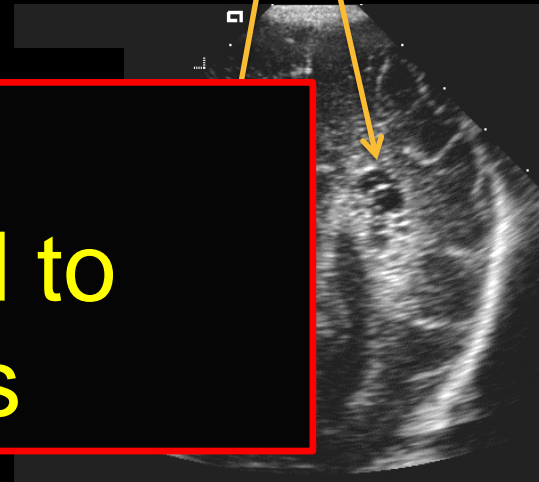
Healthy



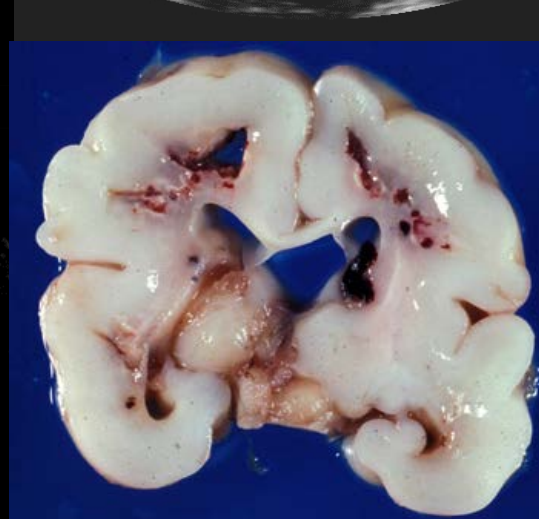
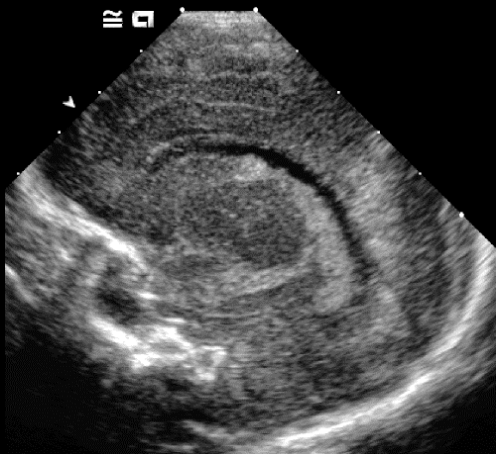
Bleeding due to hypoxia



Cysts due to hypoxia/ischemia



Brain lesions are irreversible and lead to long-term disabilities



Clinical situation today

1st days of life

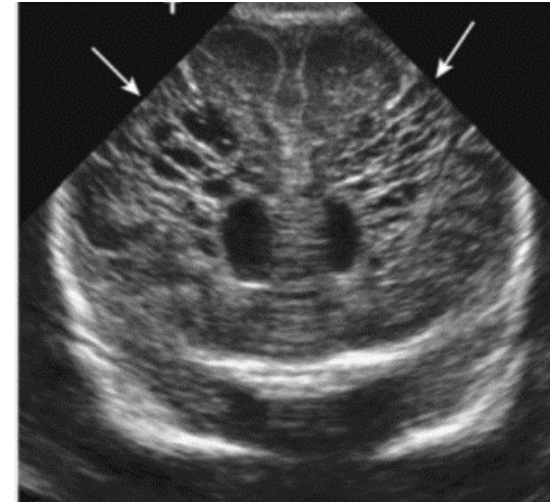


hypoxia invisible

3 weeks



22nd day of life

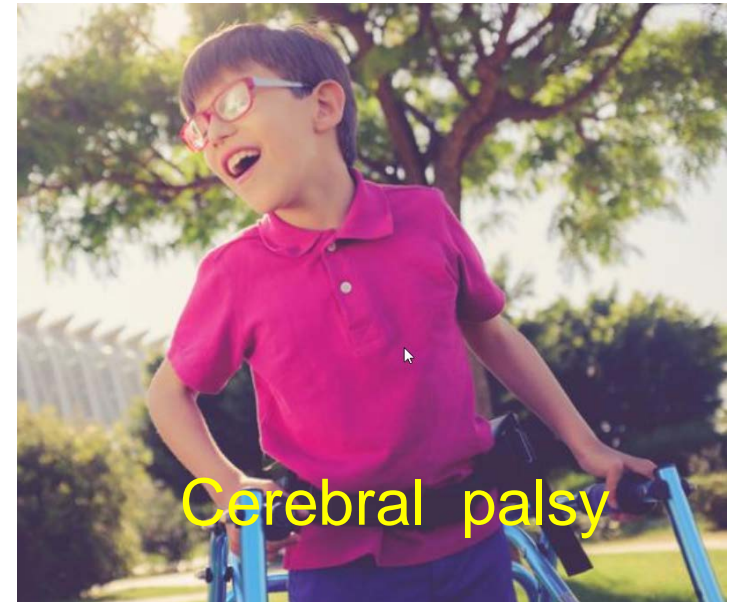


cysts due to hypoxia at $\leq 72h$

- Brain damage occurs during first 72h of life due to **hypoxia/ischemia**
- Hypoxia cannot be measured → not treated
- White matter injury visible only once tissue decays (day 21) → too late
- Irreversible brain damage → life-long disability
- **If hypoxia was detected, → prevention possible**

High clinical need to prevent brain lesions

- 900 preterm infants / year in CH (23 - 32 weeks gestation)
- 15 millions worldwide
- 80% survivors
- 50% significant cognitive delay
- 40% behavioural problems
- 25% cerebral palsy



➔ Lifelong and severe socio-economical burdens

How to prevent life-long disability:

- Needed:
 - Quantitative oxygenation imaging
 - At bedside

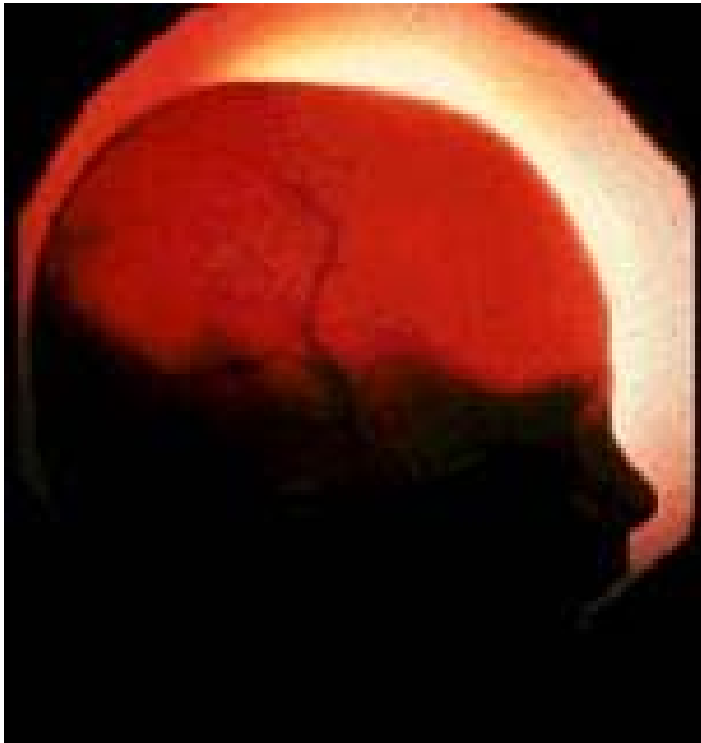
Modality	Oxygenation	Quantitative	Non-ionizing	Bed-side	Continuous	
CT	No	-	No	No	No	} risky transport
PET	No	-	No	No	No	
MRI	No	-	Yes	No	No	
EEG	No	-	Yes	Yes	Yes	} routine techniques
Ultrasound	No	-	Yes	Yes	(Yes)	
Optoacoustic	Yes	No	Yes	Yes	(Yes)	} research
NIROT	Yes	Yes	Yes	Yes	Yes	} choice

How to prevent life-long disability: *PiO*neer

- Needed:
 - Quantitative oxygenation imaging
 - At bedside

Modality	Oxygenation	Quantitative	Non-ionizing	Bed-side	Continuous	
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Ultrasound	No	-	Yes	Yes	(Yes)	
Optoacoustic	Yes	No	Yes	Yes	(Yes)	} research
NIROT	Yes	Yes	Yes	Yes	Yes	} choice

NIRS and NIROT

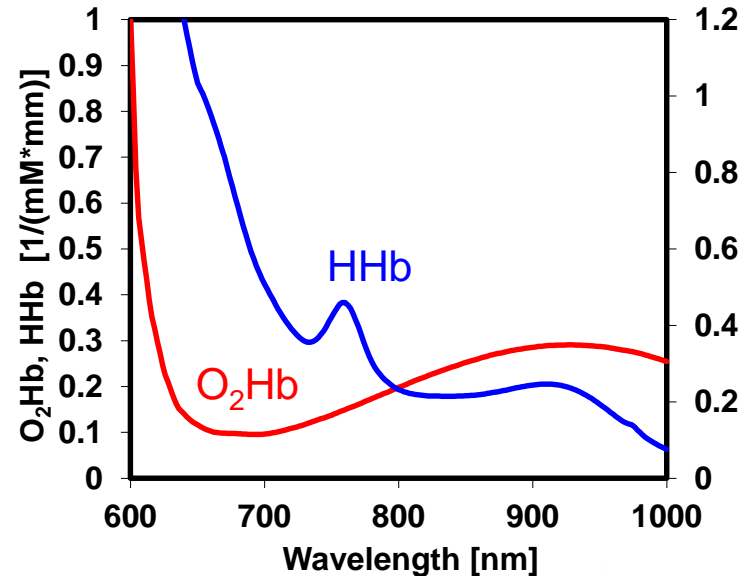


Transillumination of whole head

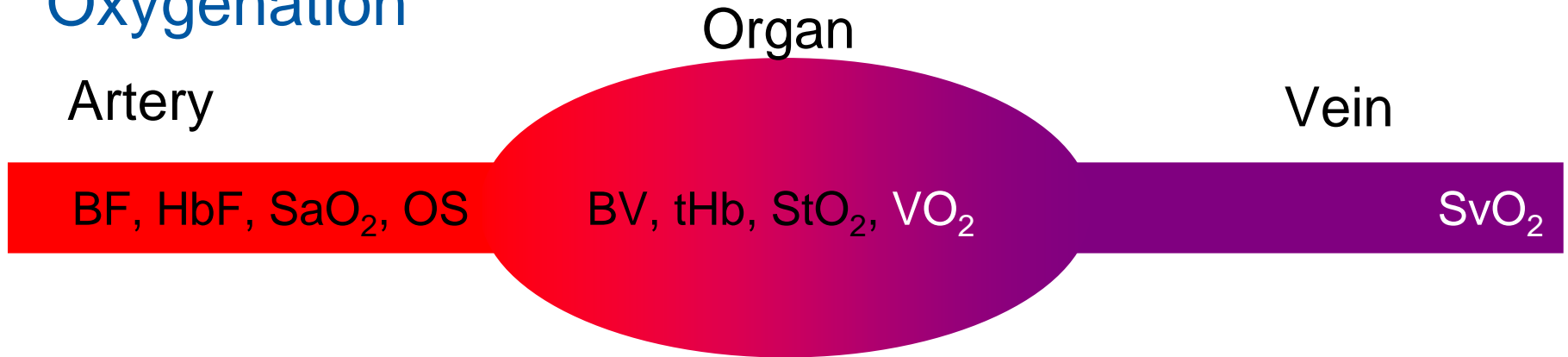
Contrast: **Oxy-**, **deoxyhemoglobin**

Oxygenation $StO_2 = O_2Hb / (O_2Hb + HHb)$

**Quantitative, non-invasive, harmless,
frequently repeatable**



Oxygenation



Blood volume BV in [ml/100g] or total hemoglobin concentration [tHb $\mu\text{mol/l}$]

Blood flow BF in ml/100g/min or hemoglobin flow HbF [$\mu\text{mol}/(\text{l} \cdot \text{min})$]

Arterial, venous or tissue oxygen saturation SaO₂, SvO₂, StO₂ [%]

O₂ delivery DO₂ [$\mu\text{mol}/(\text{l} \cdot \text{min})$] DO₂ = HbF * SaO₂

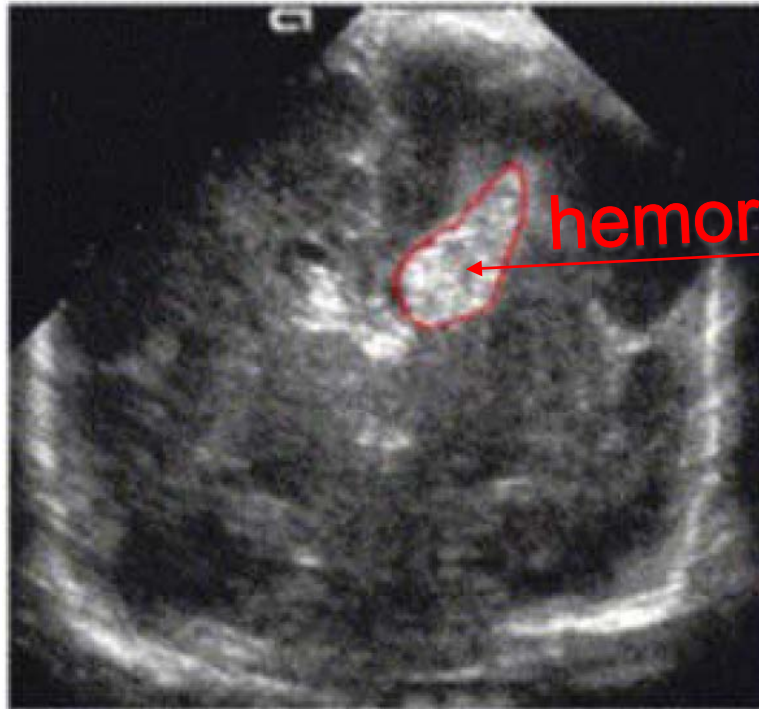
O₂ consumption VO₂ [$\mu\text{mol}/(\text{l} \cdot \text{min})$] VO₂ = HbF * (SaO₂ - SvO₂)

Tissue oxygen saturation StO₂ [%] = 0.25 * SaO₂ + 0.75 * SvO₂ ~ SvO₂

$$\text{StO}_2 = \text{SaO}_2 - 0.75 * \text{VO}_2 / \text{HbF}$$

$$\text{tHb} = a * \text{HbF}^\beta \text{ where } 0.28 < \beta < 0.38$$

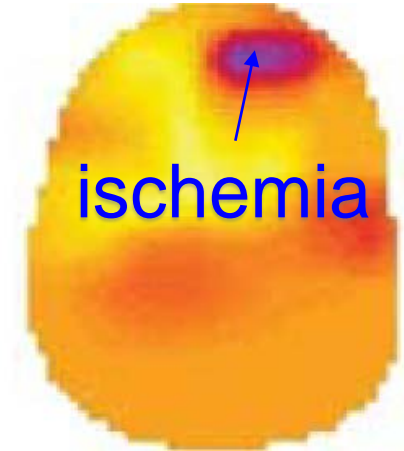
State of the art in NIROT



Blood volume



StO₂



Cooper RJ 2014 RSI 85, 053105

State of the art in NIROT

- Spatial resolution $\sim 1\text{cm}$
- ≤ 32 PMT detectors
- Bulky systems
- NOT UPSCALABLE



Cooper RJ 2014 RSI 85, 053105

State of the art in NIROT

- Spatial resolution ~1cm
- ≤32 PMT detectors
- Bulky systems
- NOT UPSCALABLE

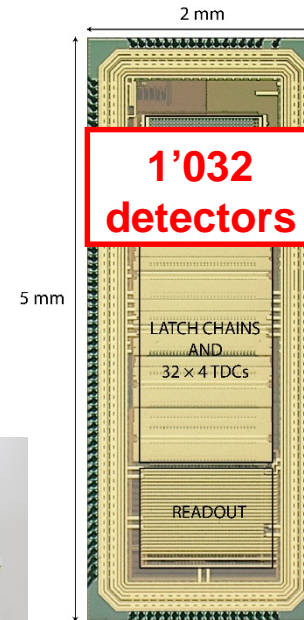
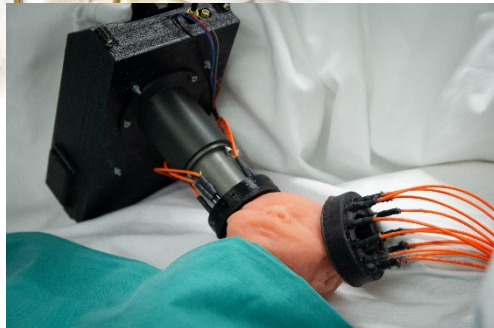


MONSTIR II



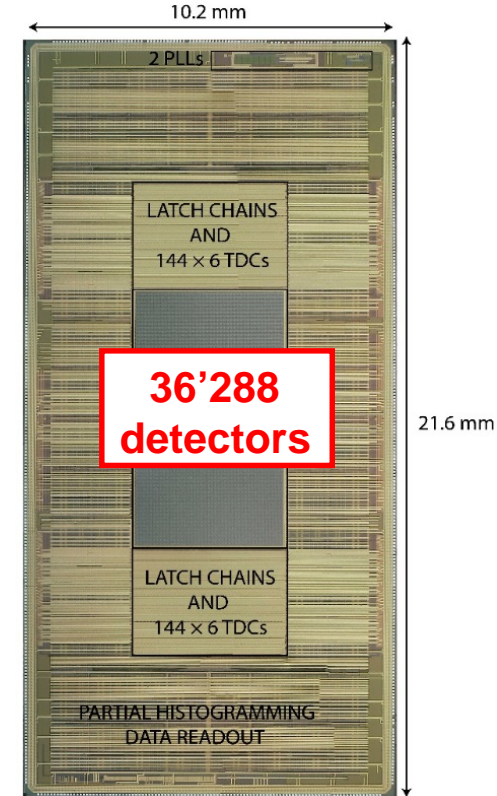
Cooper RJ 2014 RSI 85, 053105

Our approach: NIROT Pioneer



Piccolo
32 × 32

SPAD image sensor
(128 timestamps per frame)



Ocelot

144 × 252

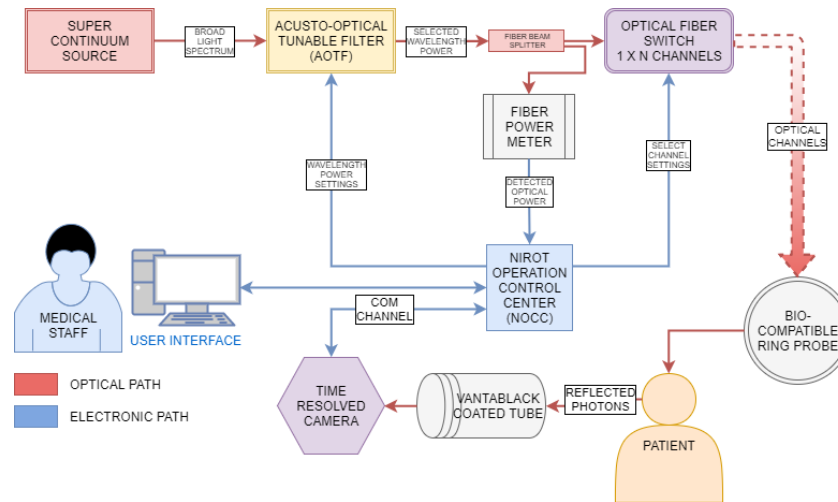
SPAD image sensor
(1726 timestamps per frame)

- Single-photon SPAD time-resolved picosecond camera
- ~1000 x more detectors than state of art

Ocelot and Piccolo

	Ocelot	Piccolo
Array size	144 X 252	32 X 32
DCR Hz	60	141
Fill-factor %	28	28
Peak PDP (500nm) %	40	40
PDP NIR (800nm) %	12	12
Microlenses CF	2.97	2.97
PDE (800nm) %	10	10
Max. excess bias V	5.5	5.5
No. of TDCs	1728	128
TDC LSB ps	48.9 or 65.1	48.9
FWHM timing response (ps)	116	116
1/0 bandwidth Gbps	11.5 Gbps	5.12
Max. throughput Gphotons/s	6 Gphoton/s (includes compression)	0.224
Die area mm ²	10.3 mm x 21.6 mm	2.0 mm x 5.0mm

Schematic of the Pioneer system



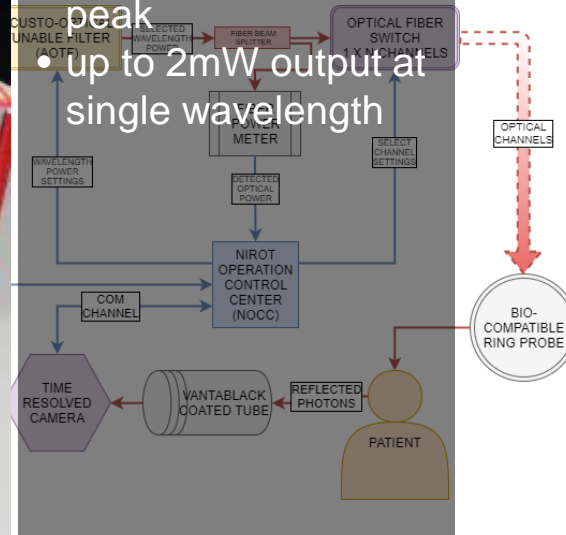
Schematic of the Pioneer system



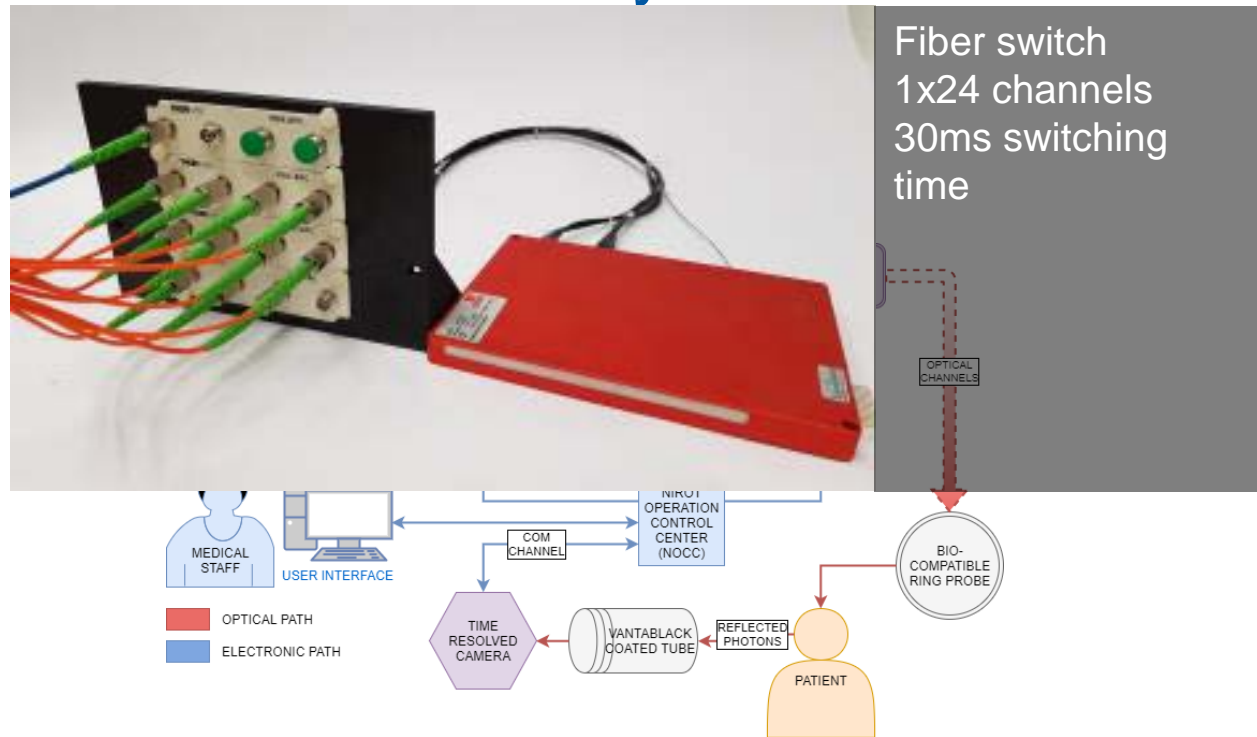
Fianium WL-450-8

- 8W total output
- 650-950nm range
- ~5-10nm FWHM peak

- up to 2mW output at single wavelength



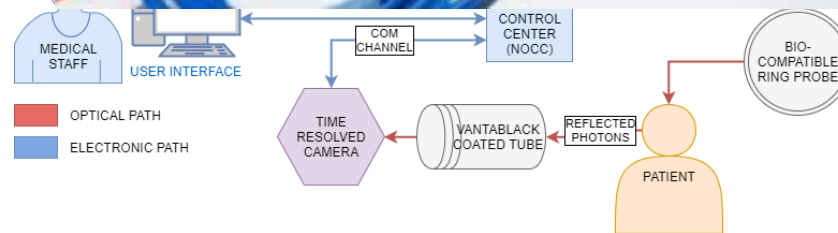
Schematic of the Pioneer system



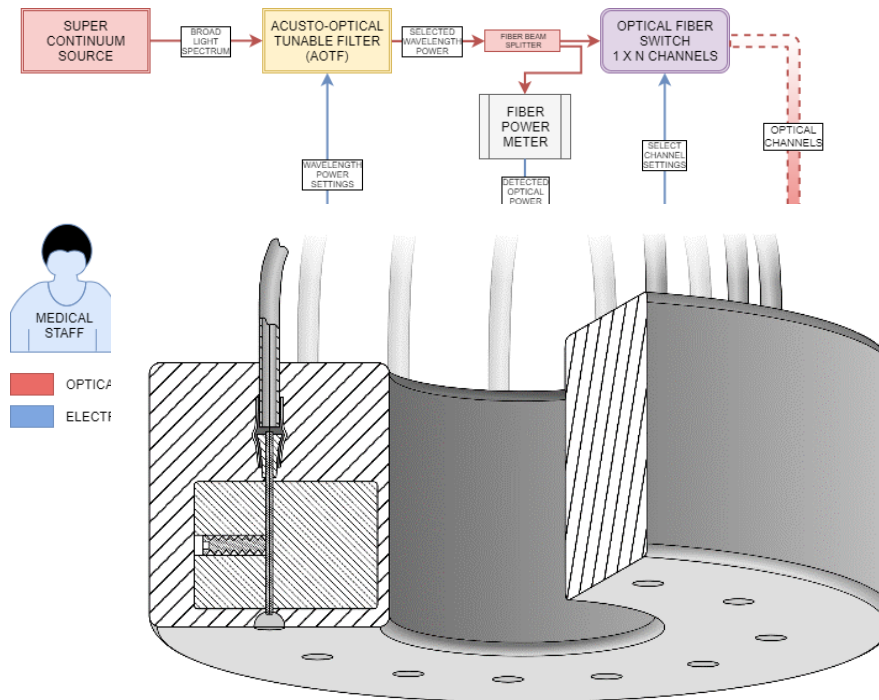
Schematic of the Pioneer system



Y-fiber splitter with power meter
98/2 splitting ratio

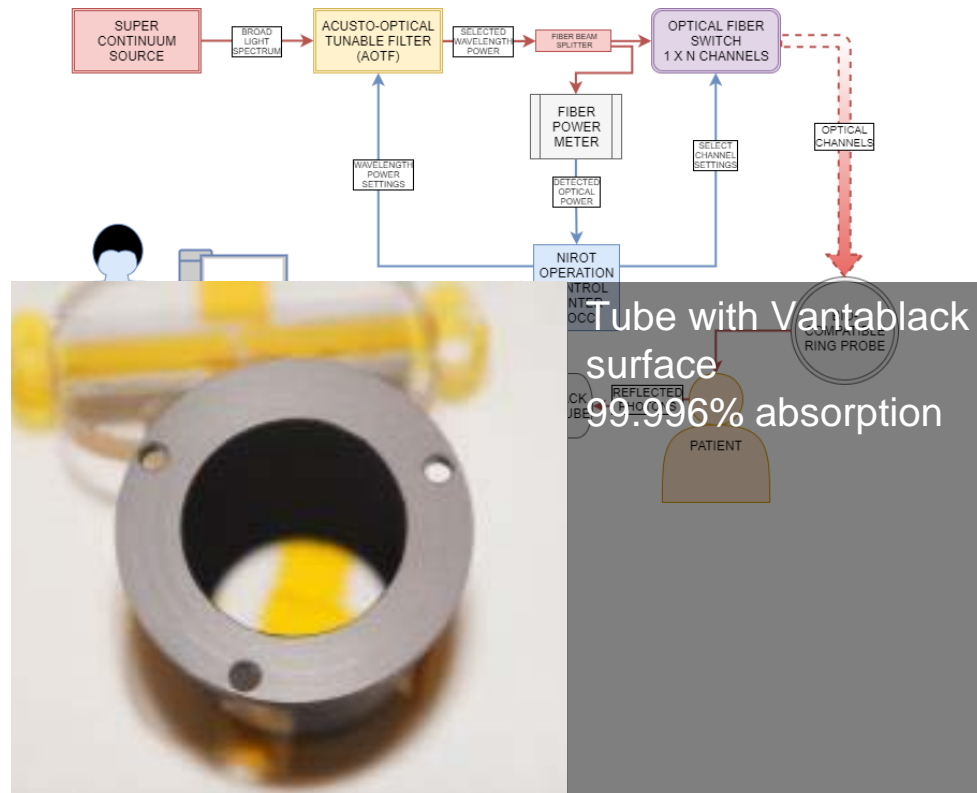


Schematic of the Pioneer system

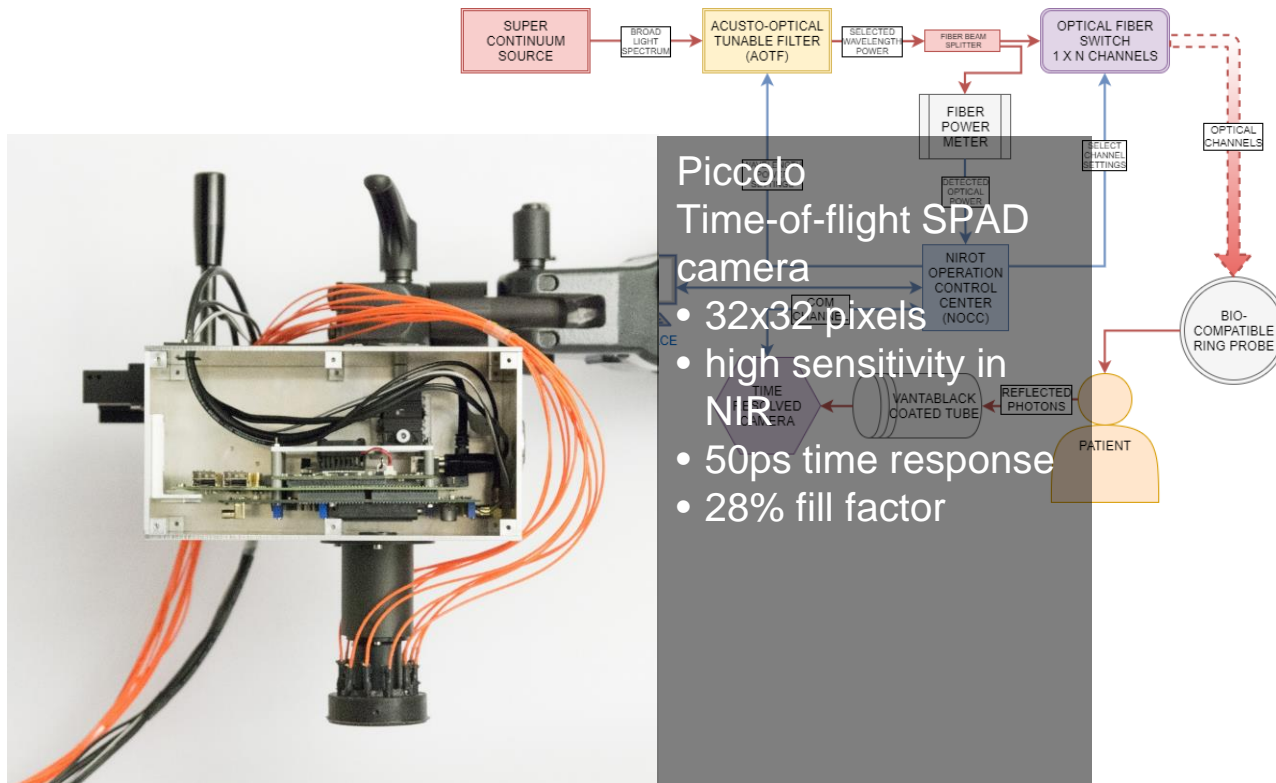


- Source ring
- 11 optical sources
 - biocompatible
 - 25mm FoV

Schematic of the Pioneer system

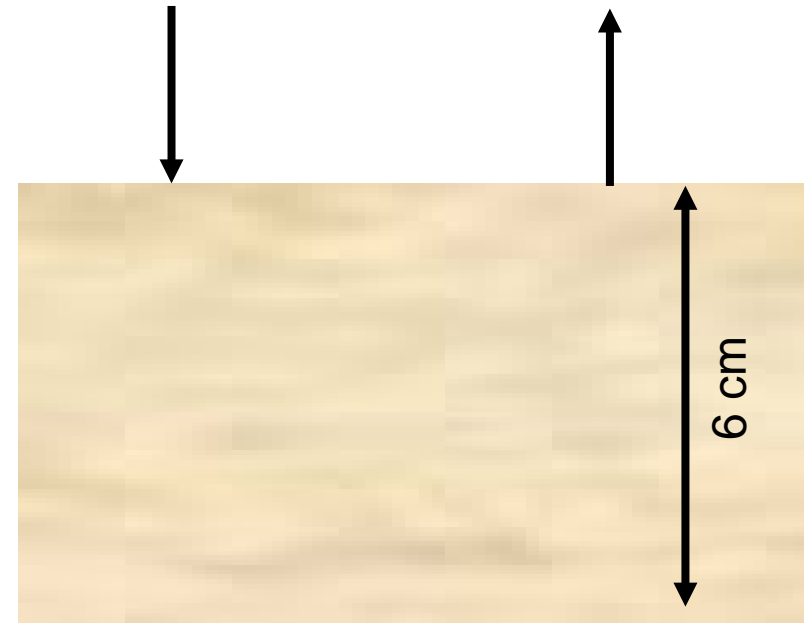
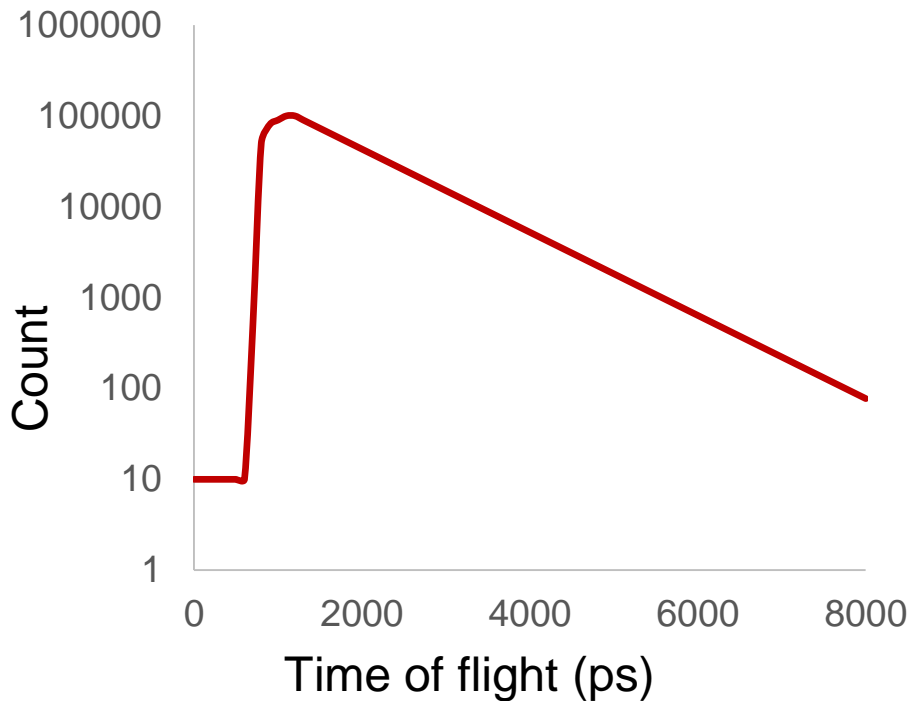


Schematic of the Pioneer system



Picosecond timing resolution

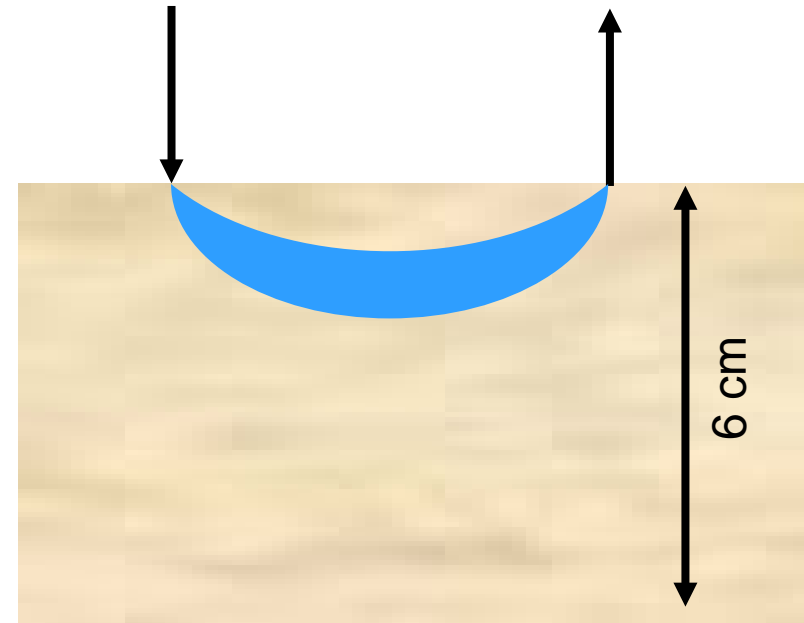
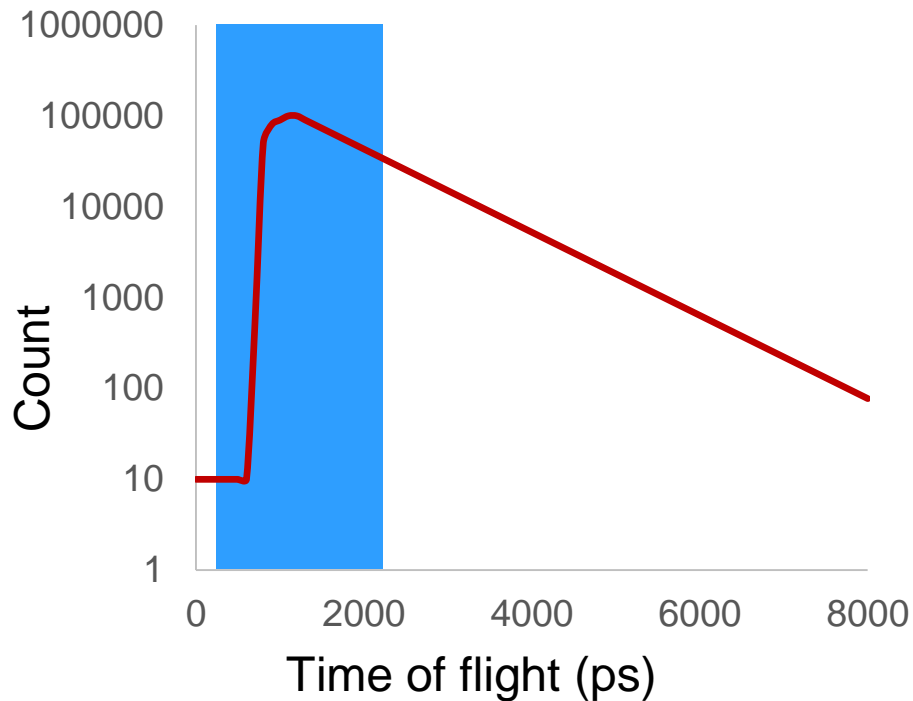
- Depth reachable and clinical usefulness
 - 6cm for gated SPAD, ~zero distance



Tosi A et al. Opt Exp 2011;19:10735-46

Picosecond timing resolution

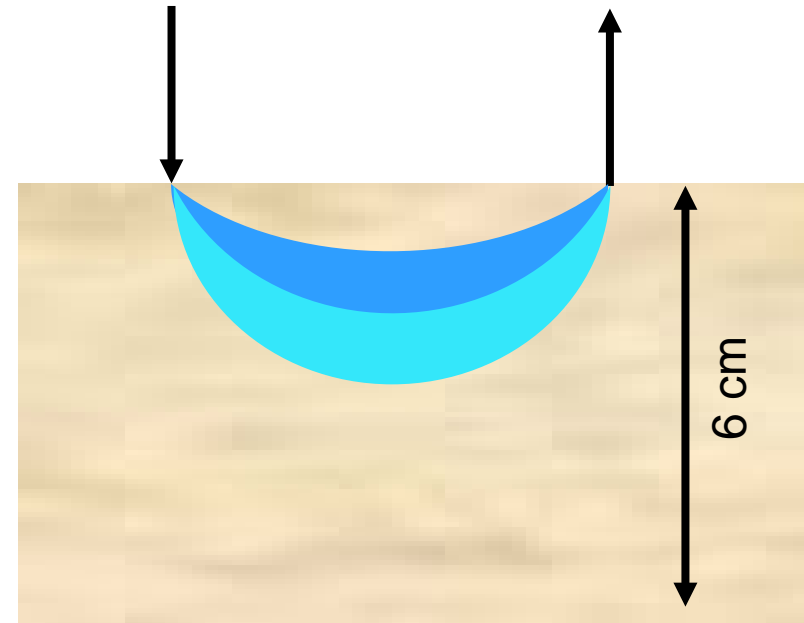
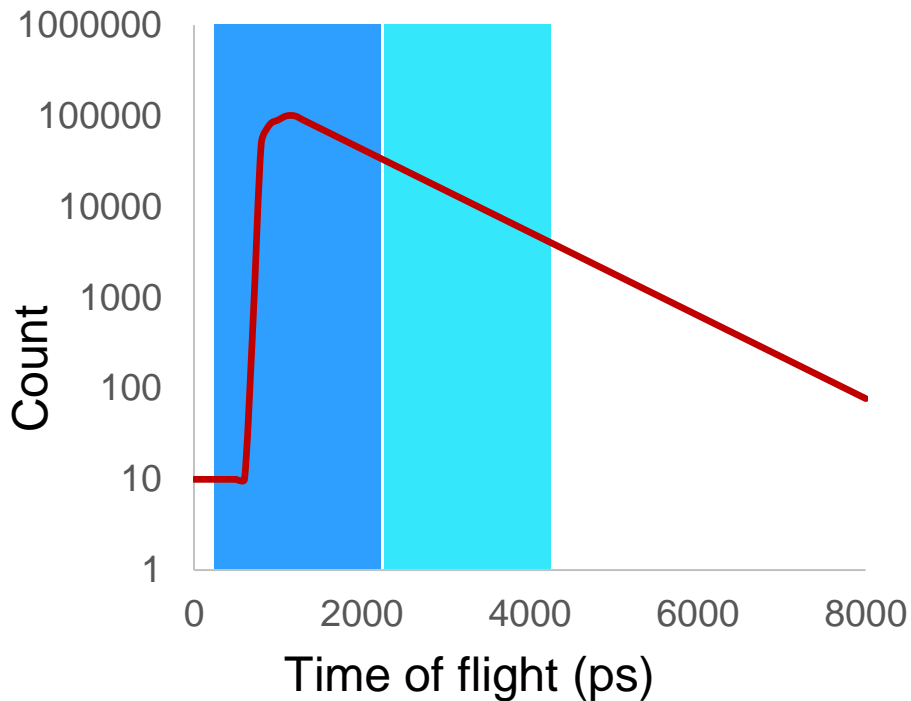
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Tosi A et al. Opt Exp 2011;19:10735-46

Picosecond timing resolution

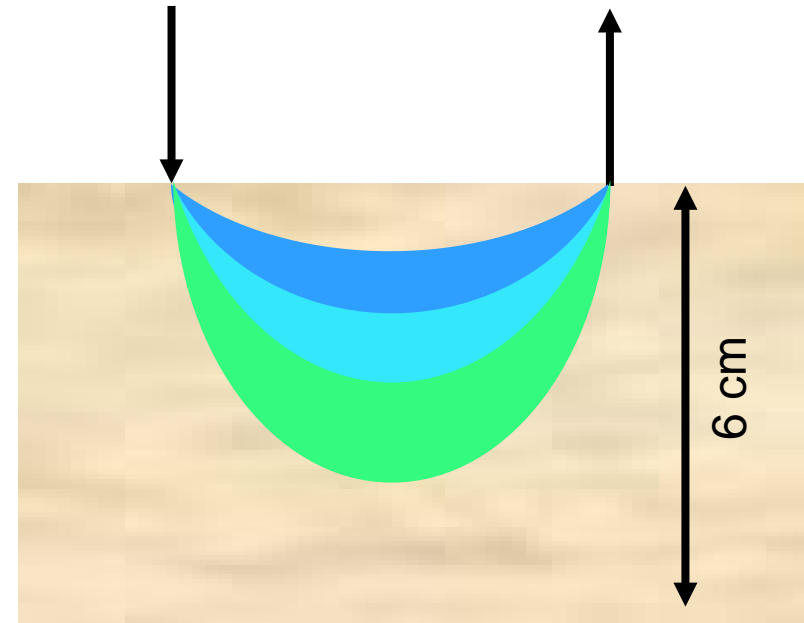
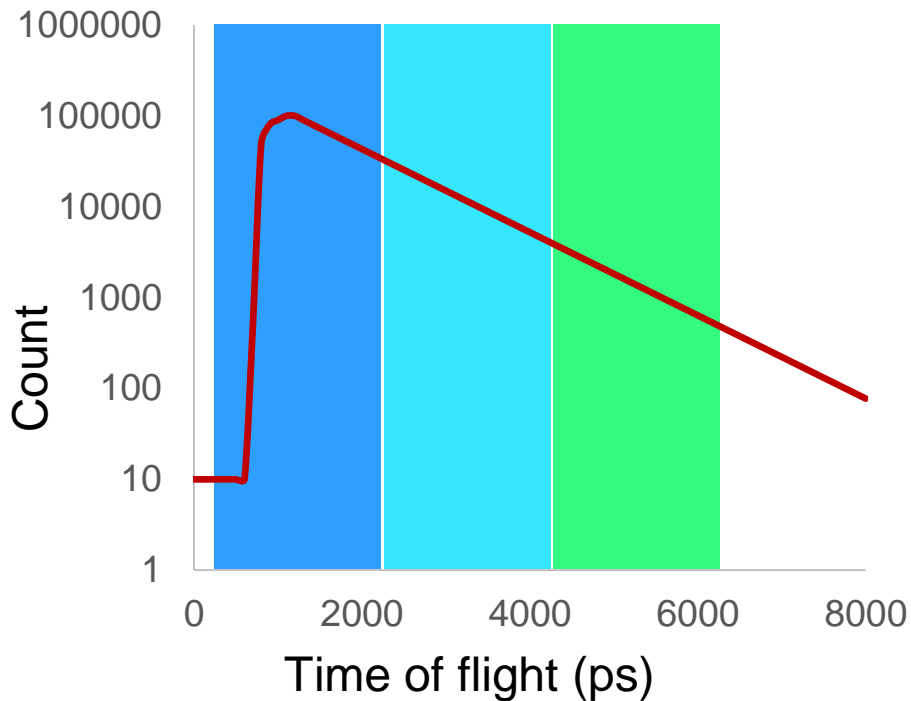
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Picosecond timing resolution

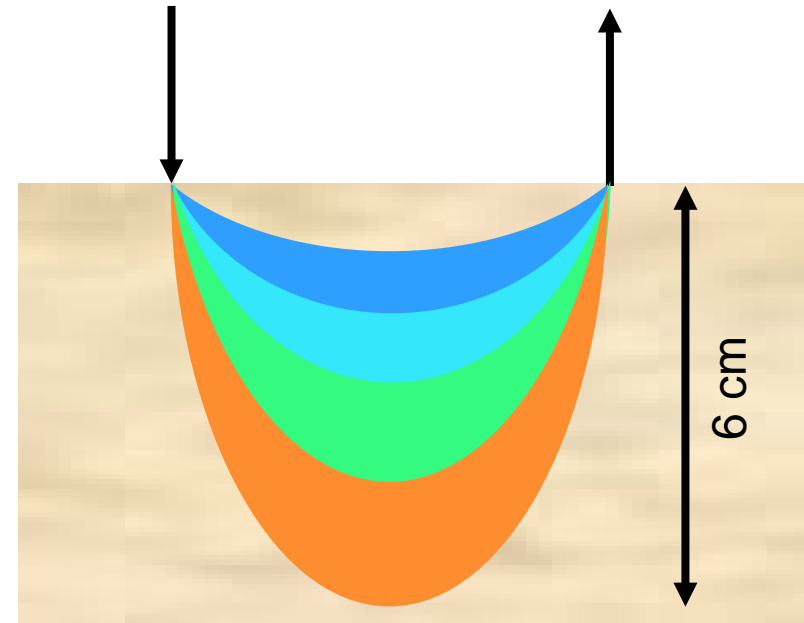
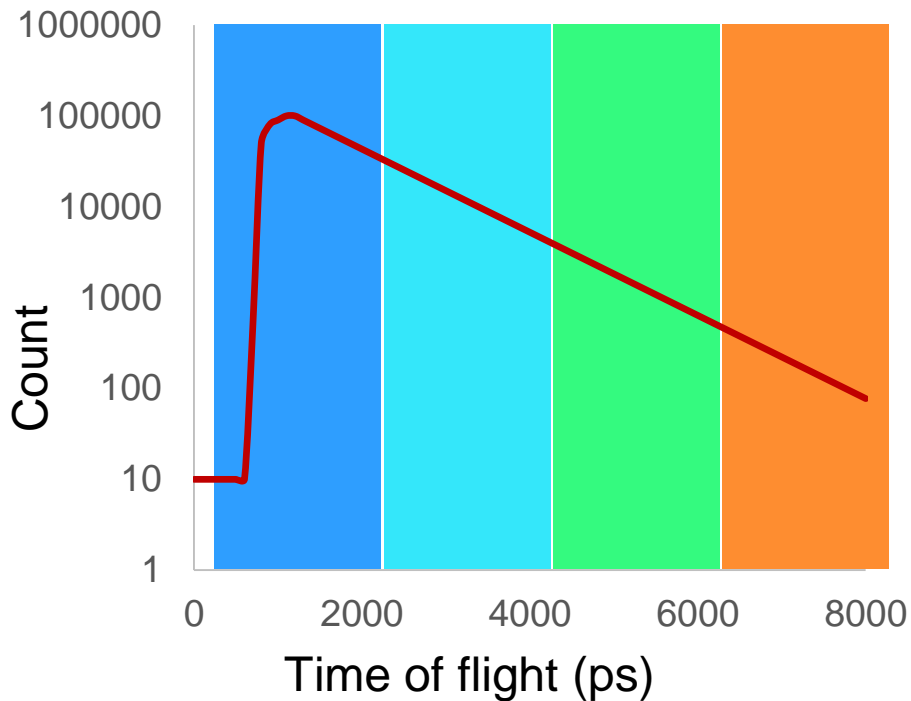
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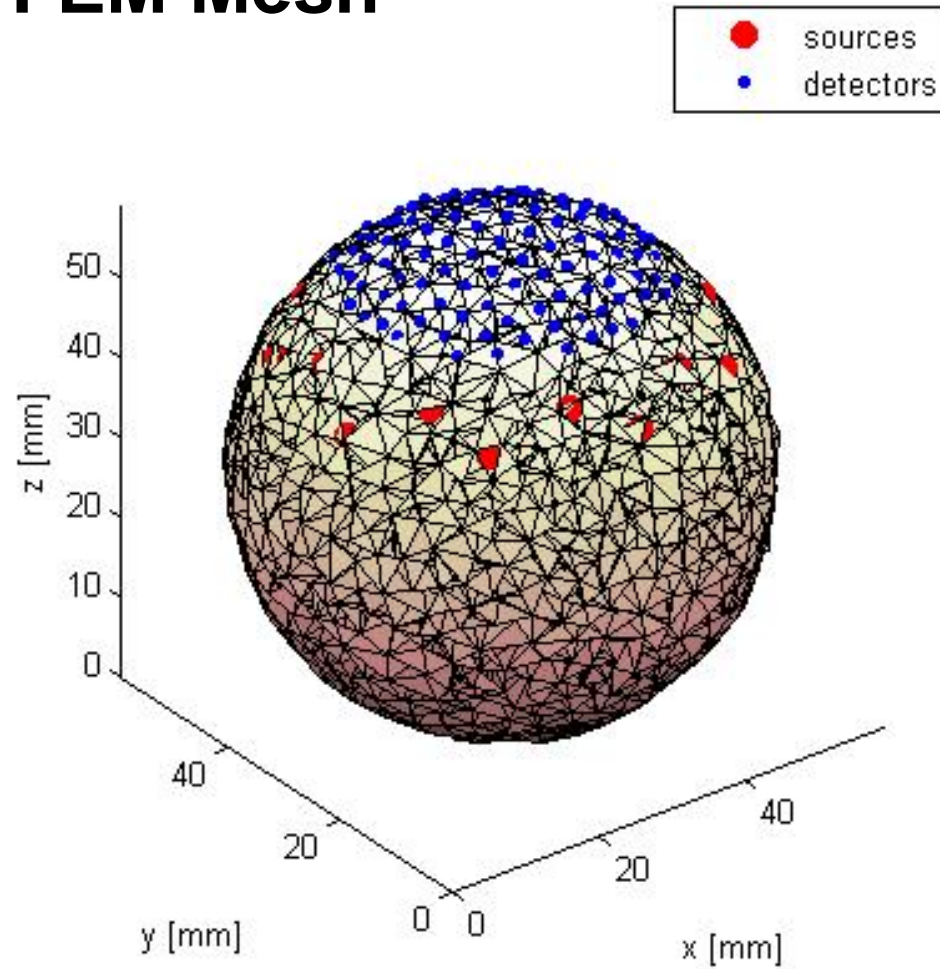
Picosecond timing resolution

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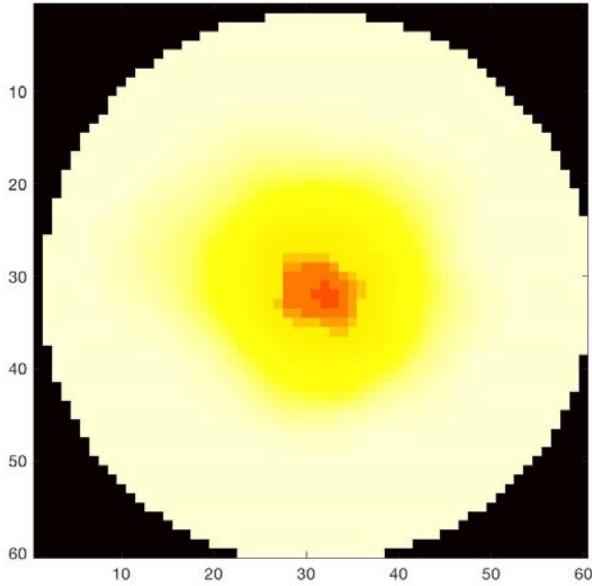
Tosi A et al. Opt Exp 2011;19:10735-46

FEM Mesh



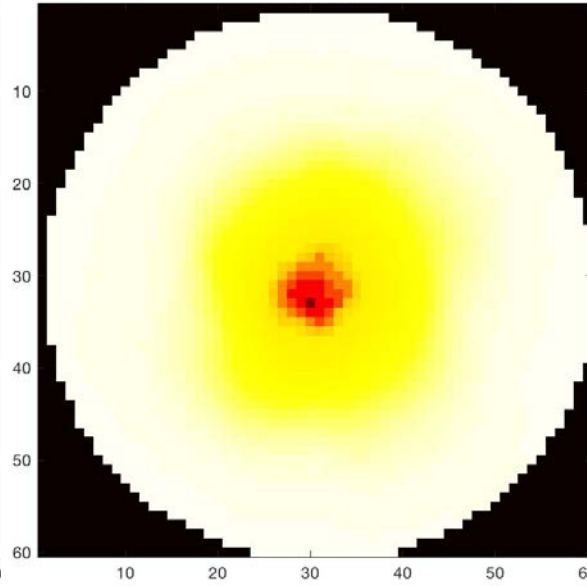
Simulation results

Ischemia 1.8mm \emptyset



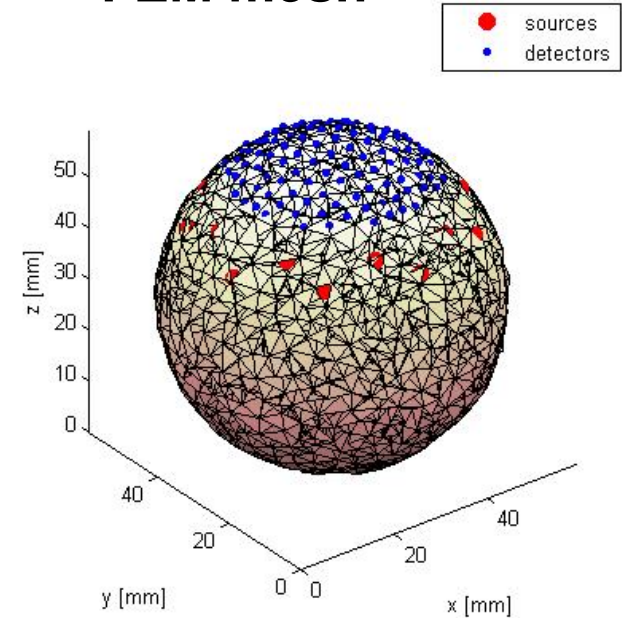
Contrast factor 250%

Bleeding 1.8mm \emptyset



Contrast factor 5000%

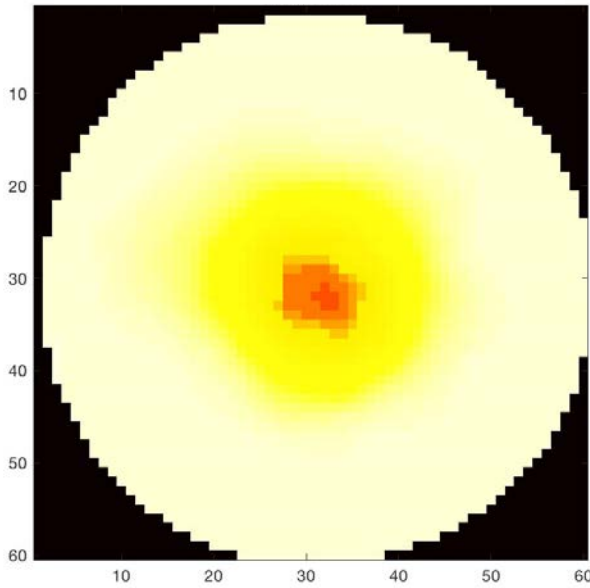
FEM mesh



Lesions of 1.8mm diameter detectable

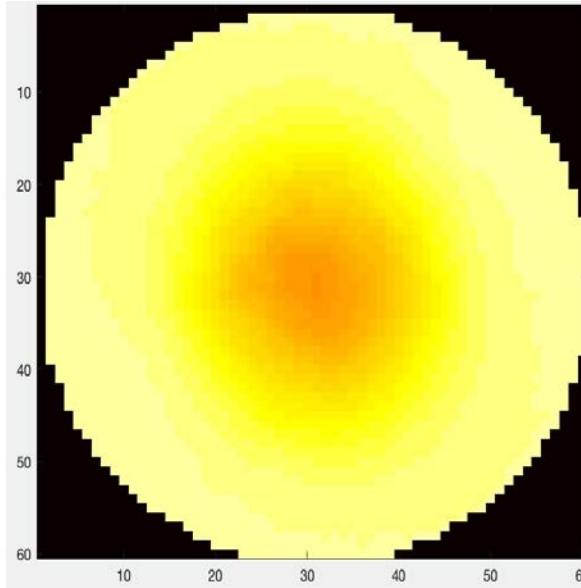
Simulation results

Ischemia 1.8mm \emptyset



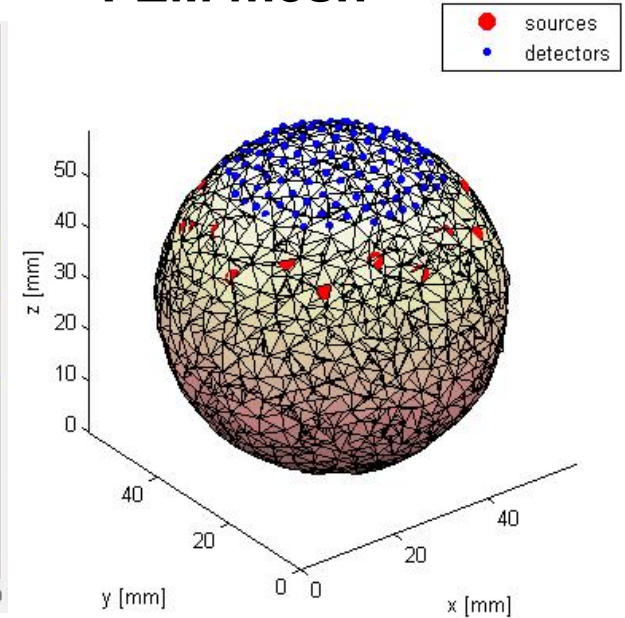
116 detectors

Ischemia 1.8mm \emptyset



32 detectors

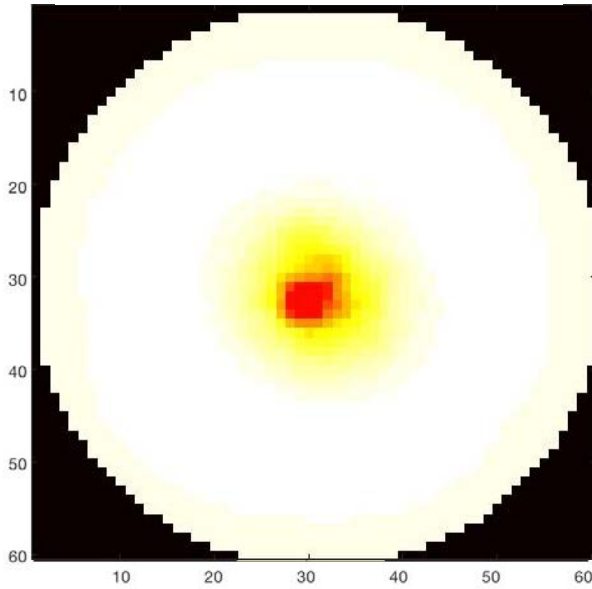
FEM mesh



Number of detectors increases the resolution

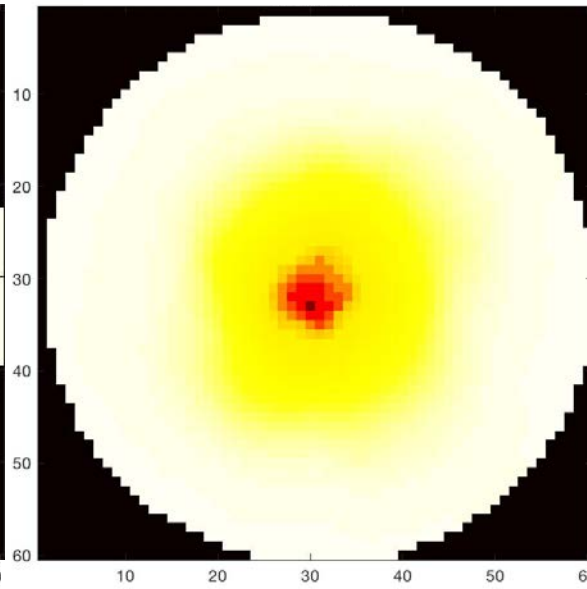
Experiment vs. simulation results

Bleeding 1.8mm \emptyset



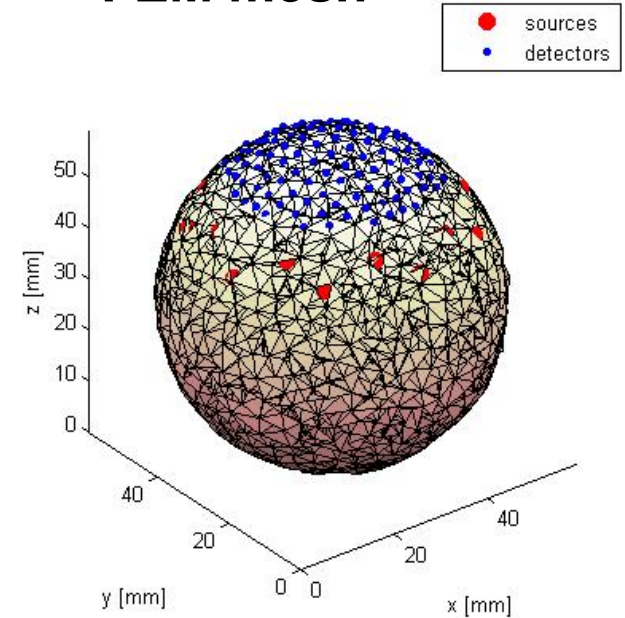
Experiment

Bleeding 1.8mm \emptyset



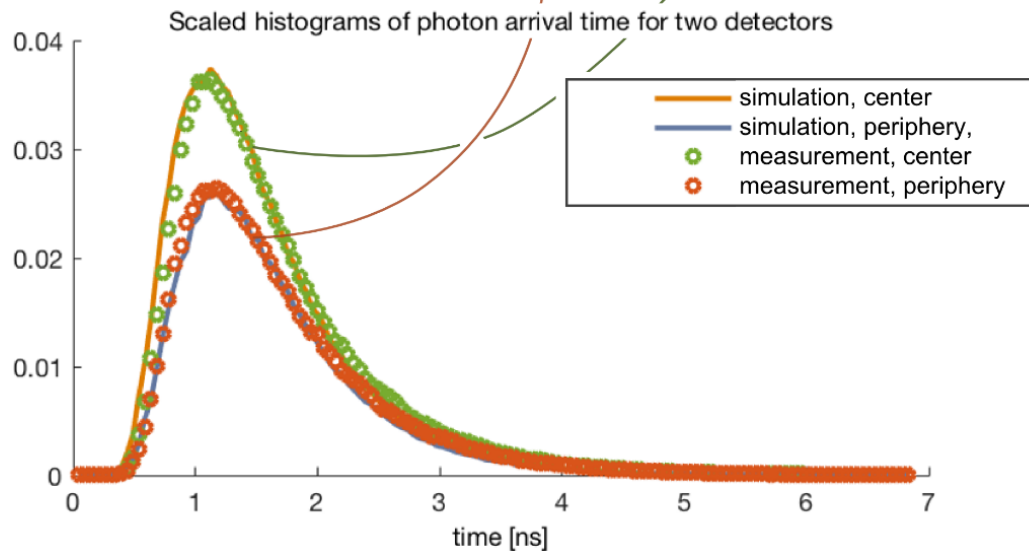
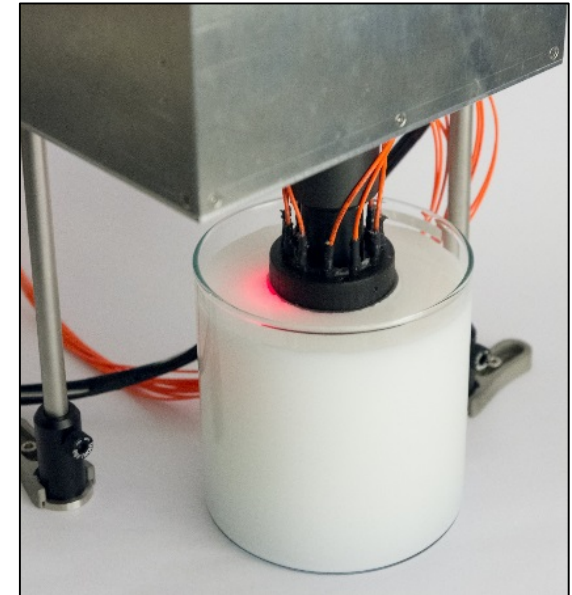
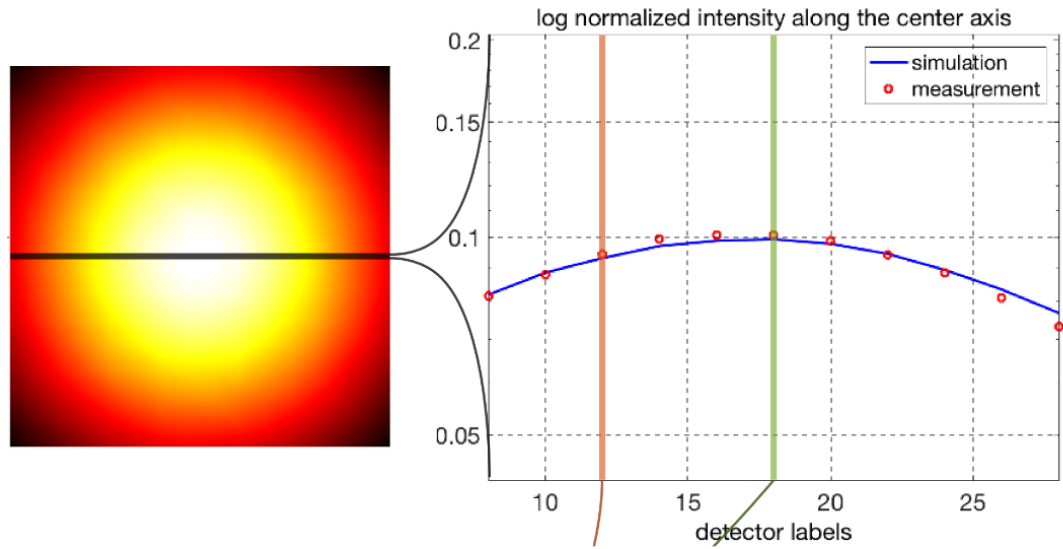
Simulation

FEM mesh

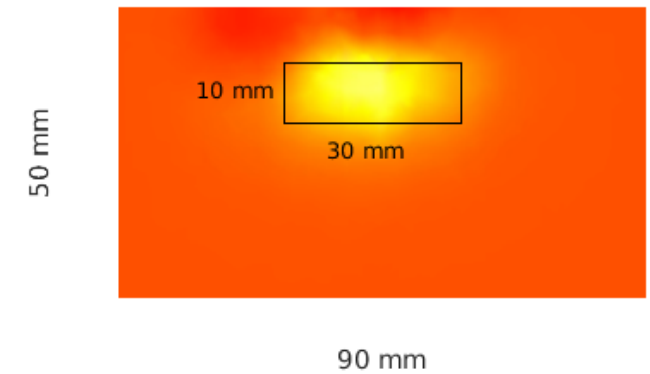
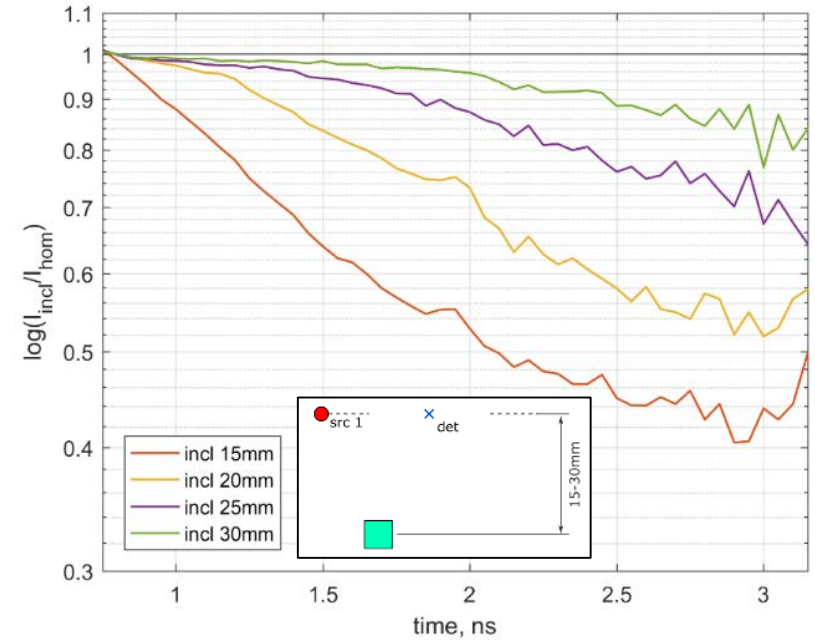
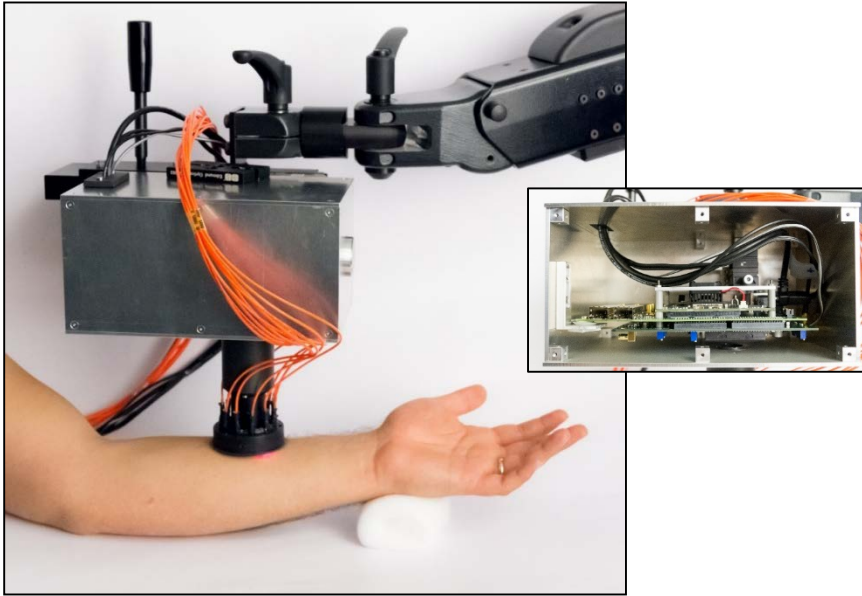


Experiment and simulations agree

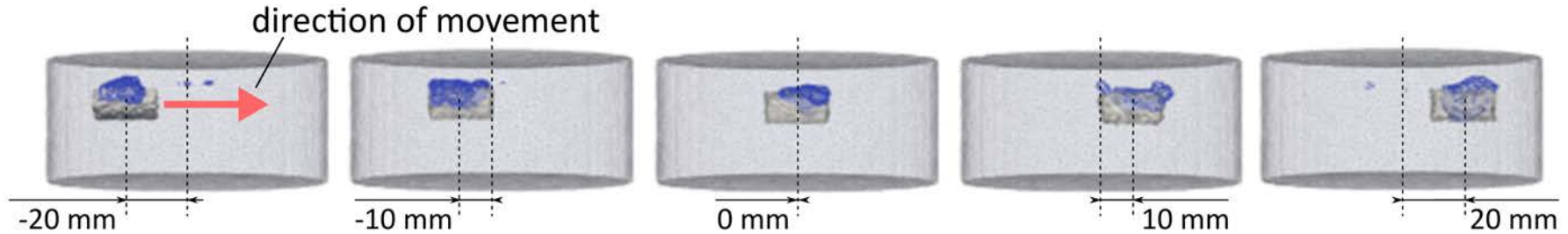
Phantom results



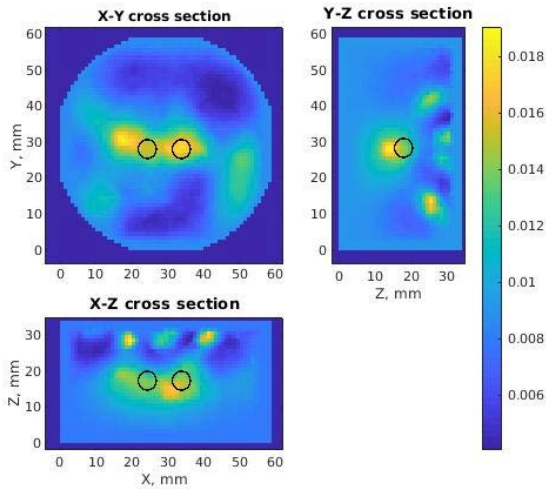
HR-NIROT prototype & results



Phantom validation: Speed



Tracking objects
0.2 second acquisition / source



Case 1: resolution
Two spheres $\varnothing = 5$ mm
lateral distance = 5 mm
depth = 15 mm

When it comes to clinics ...

- Moles and hair are difficult to model
- Instrumental response function is non-trivial to decouple

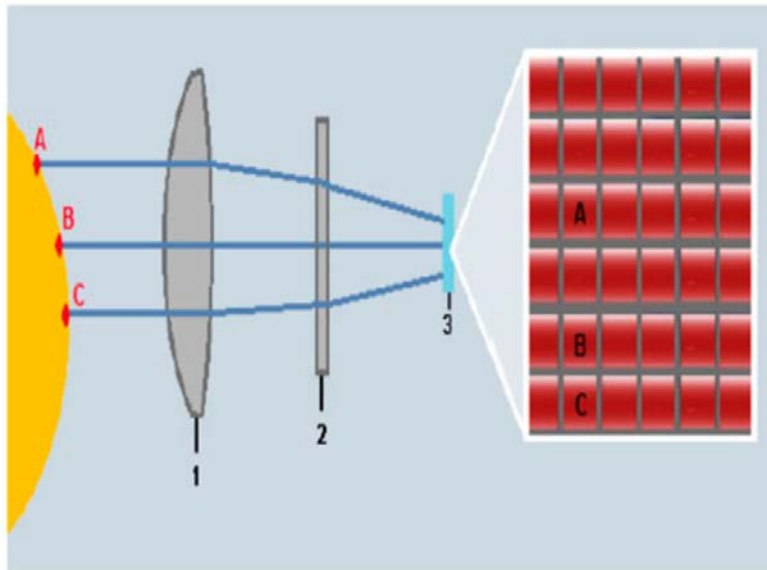
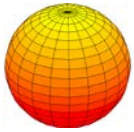


Fig.1 Three rays A, B and C are projected from the object to the SPAD array.

- Methods needed to tackle noise: Calibration methods

J. Jiang, M. Wolf, and S. Sanchez Majos, "Fast reconstruction of optical properties for complex segmentations in near infrared imaging," J. Mod. Opt. 64, 732–742 (2017).



Phantom experiment

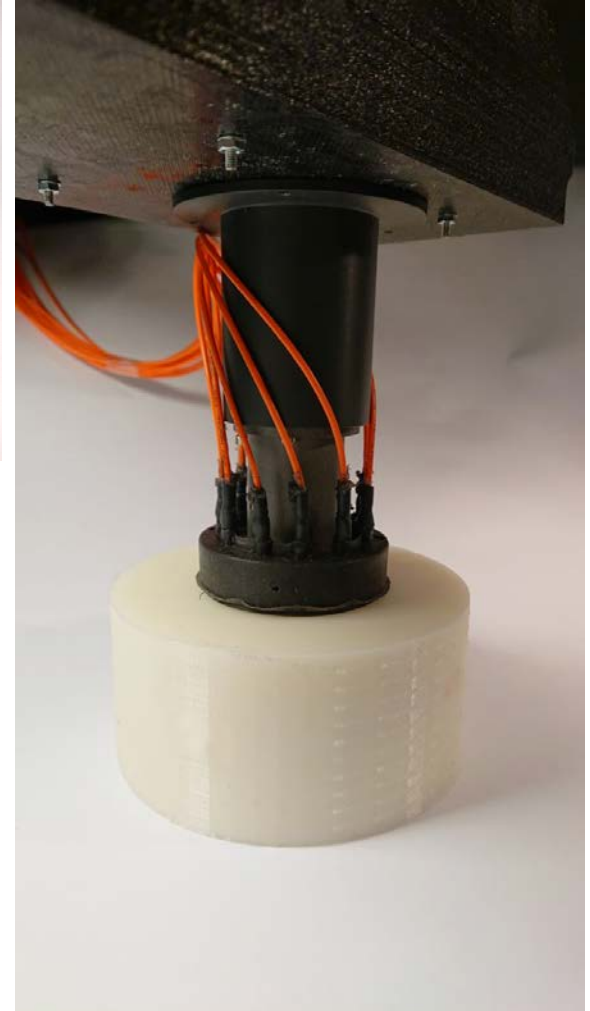
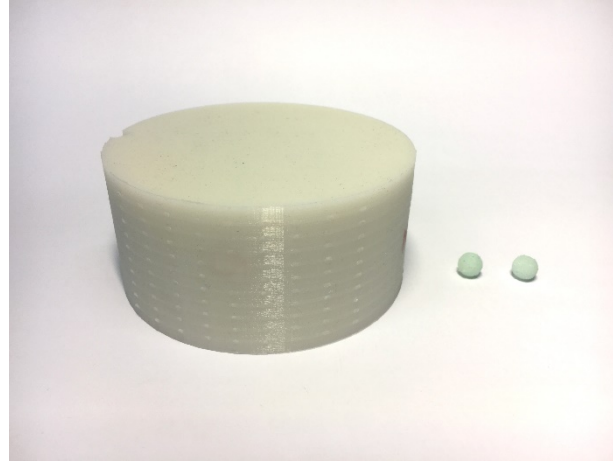
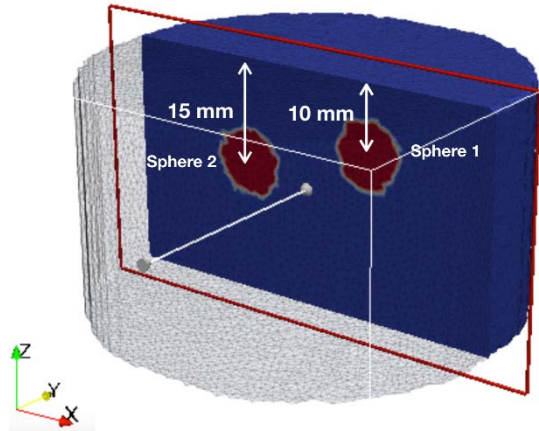
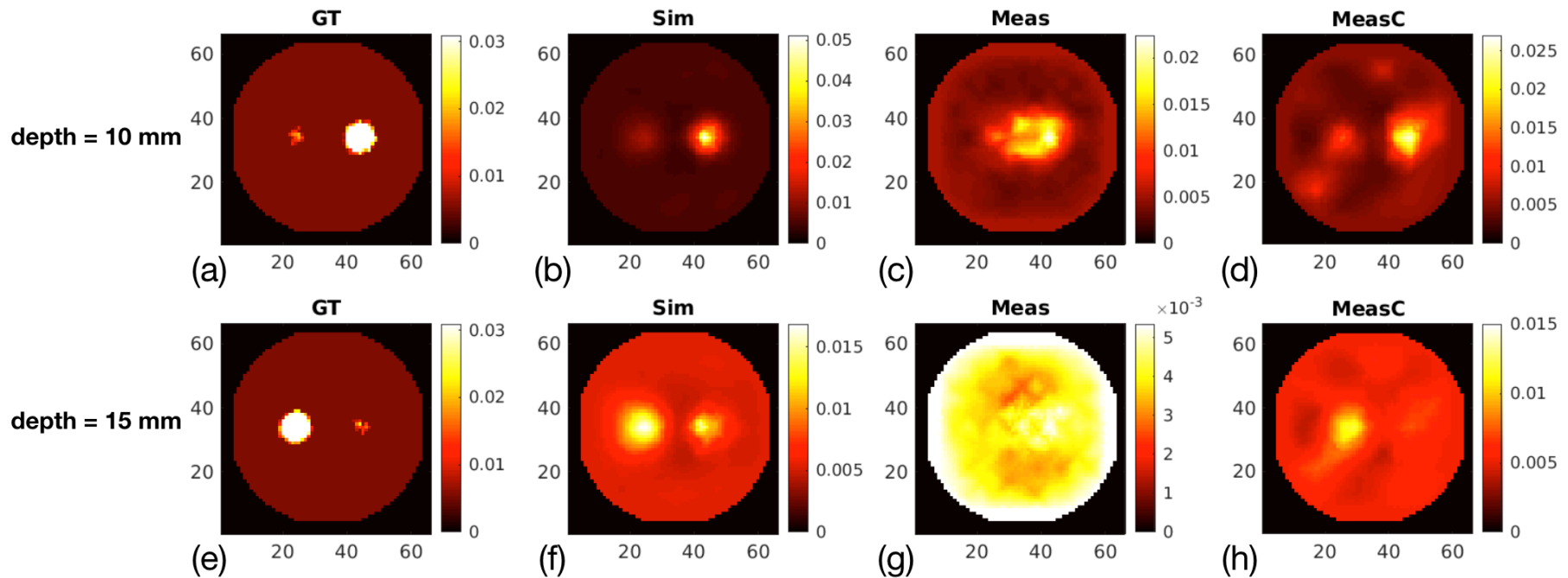
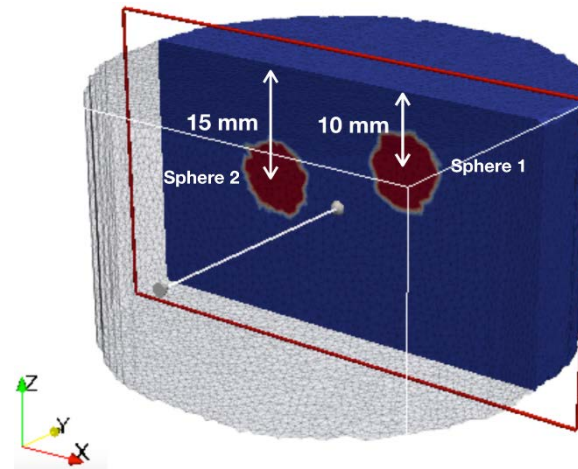


Table 1. Optical properties of the silicone phantom

optical properties	μ_a [mm^{-1}]		μ'_s [mm^{-1}]	
	689 nm	725 nm	689 nm	725 nm
wavelengths	689 nm	725 nm	689 nm	725 nm
bulk	0.0053	0.0055	0.9	0.86
sphere 1	0.031	0.025	1.06	1.01
sphere 2	0.031	0.025	1.06	1.01

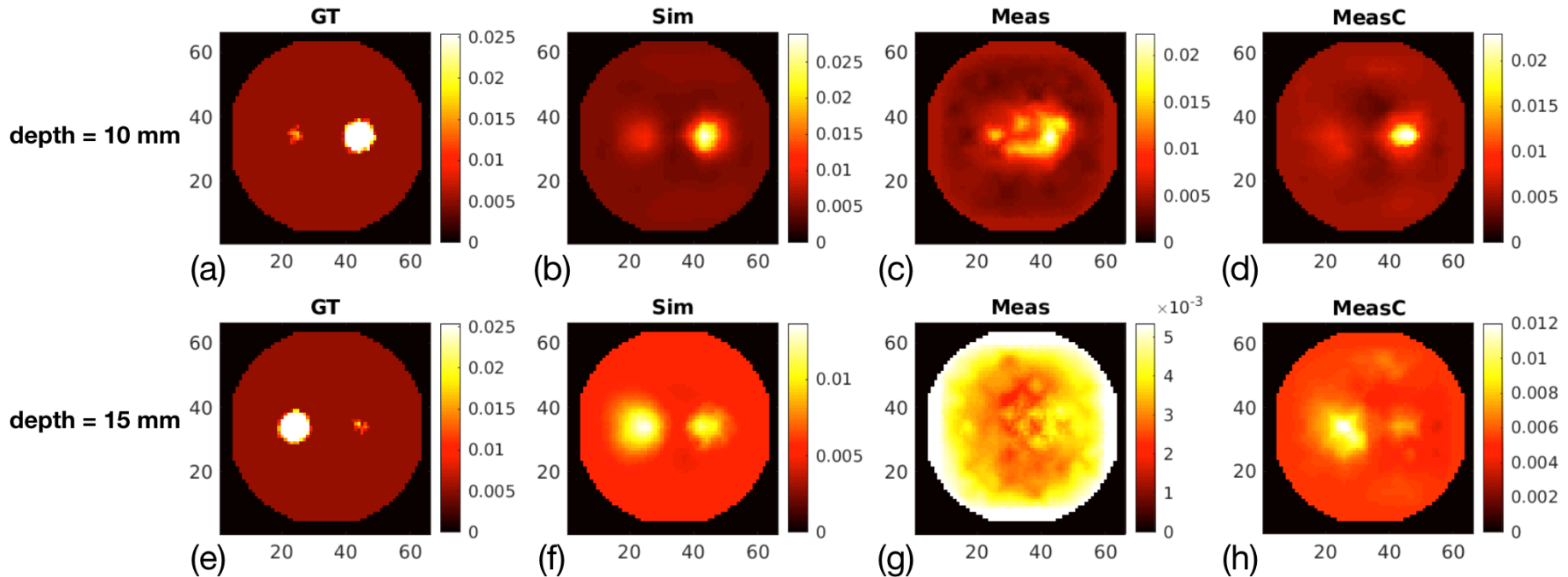
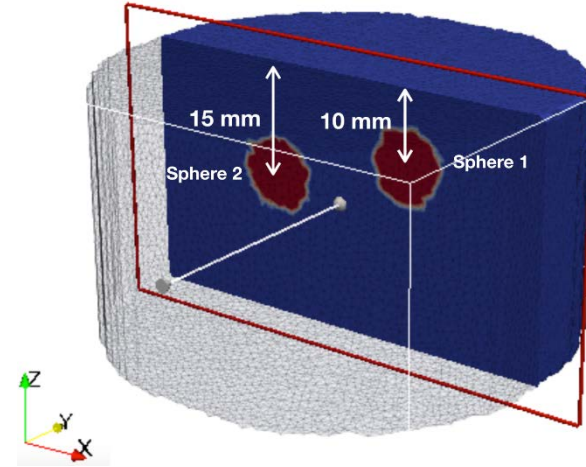
Results image reconstruction (1)

689 nm

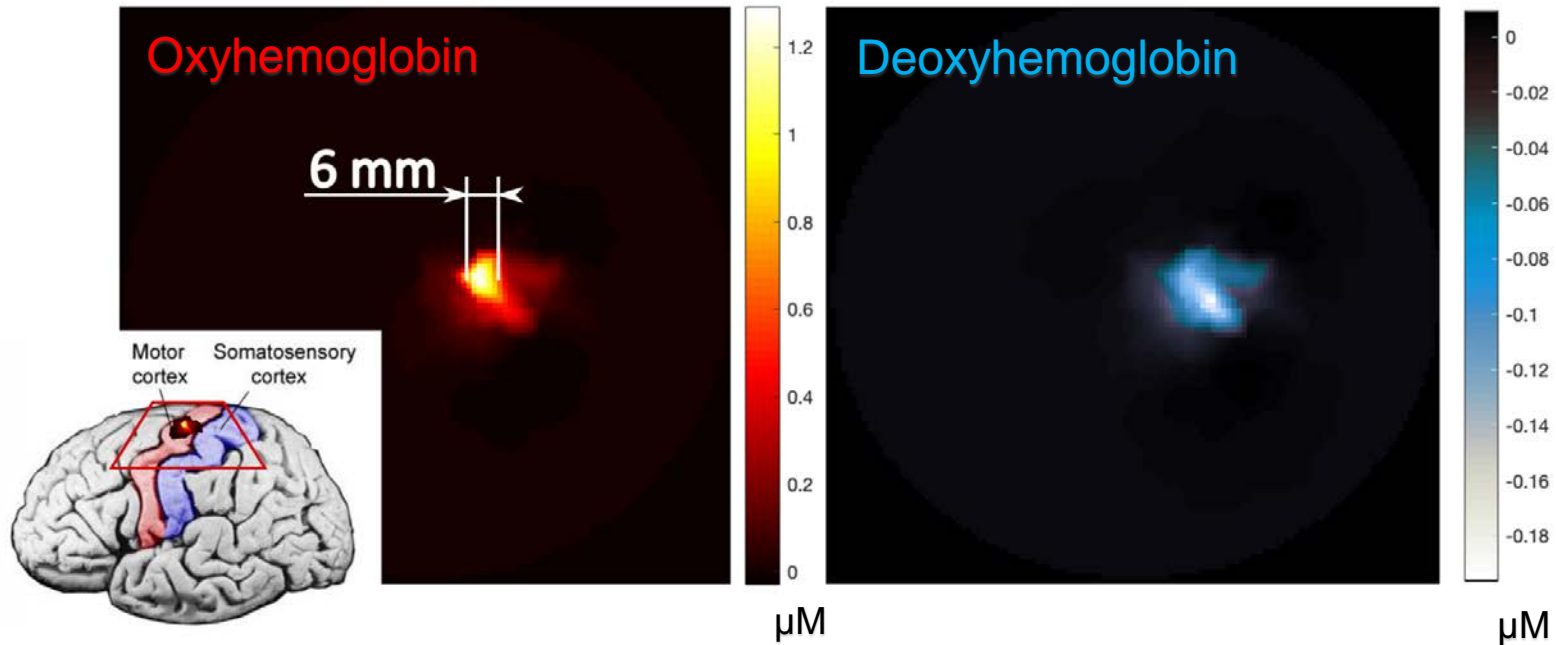


Results image reconstruction (2)

725 nm



Motor activation in adult subject



- Stimulus: Fingertapping exercise
- 3D tomographic images
- Activation visible in 2cm depth
- Demonstrates brain imaging.



Conclusions NIROT

Technological

- ✓ A new NIROT concept
- ✓ First test successful

Societal/Clinical

- ✓ 10% preterm birth rate
- ✓ Prevention & efficient therapy
- ✓ Reduced mortality & life-long disability

Outlook

- ✓ First in vivo studies
- ✓ Ocelot image sensor



Thank you!